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Vaporized Hydrogen Peroxide: A Well-Known Technology with a New Application

written by

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Abstract

Hydrogen peroxide has a multitude of uses and the vapor form was first identified as a sterilant in late 1970s. Following a number of developments, vaporized hydrogen peroxide (VHP) became widely adopted in early 90s as a substitute for ethylene oxide (EO) in device and instrument processing and reprocessing in healthcare facilities. Often VHP was hailed as the replacement technology for EO. Because of key limitations such as scale, penetration, and compatibility with packaging materials, adoption to terminal sterilization of single-use devices has not commenced to any significant level. However, recent developments in sterilization chamber design and process development provide new opportunity for consideration. For future products, such as those that require "end of production line sterilization," such limitations may be reconsidered and overcome. This article describes those challenges and how they have been addressed, with practical examples. The development of global consensus standards and leveraging the well-established knowledge of VHP sterilization with regard to microorganism inactivation and material compatibility will help facilitate wider consideration of VHP technology as a true alternative to EO in certain product applications.

Introduction – Terminal Sterilization of Medical Devices

Terminal sterilization of single-use medical devices may be broadly subdivided into two main technologies, namely radiation and sterilization by ethylene oxide (EO) gas.^[1] The continued reliance on EO is a consequence of its wideranging material compatibility and availability for scale-up. The challenges of using EO relate to the hazardous and carcinogenic nature of the gas coupled with the prolonged treatment times. Radiation, on the other hand, is a relatively guick process with no toxic residues, but is limited by the availability of the radiation source (cobalt, in the case of gamma irradiation) and material compatibility, described in AAMI TIR17.^[2] Therefore, a continual need for extension of the available terminal sterilization technologies remains and was highlighted in 2019 with the launch of the Food and Drug Administration (FDA) Innovation Challenge to identify new sterilization methods and technologies. Given its extensive history in healthcare processing and being deemed a Category B sterilization method by FDA, vaporized hydrogen peroxide (VHP) is now being considered as such a candidate technology for inclusion.



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Vaporized Hydrogen Peroxide

With hydrogen peroxide established as a biocidal agent since the 1800s and the first uses of the vapor form in sterilization emanating from the late 1970s, VHP is a well-established sterilization method of choice in the healthcare setting for the processing of reusable devices.^[3] Furthermore, VHP is used in many other applications, such as room and facility decontamination.^[4] The disinfection and sterilization efficacy of hydrogen peroxide in both aqueous and gas form are well documented,⁴,⁵ with the latter form considerably outperforming the liquid system.⁴,⁶ It has been suggested that VHP can penetrate the three-dimensional protein structure and cause breaking of bonds between subunits more easily than liquid hydrogen peroxide.^[7] The International Agency for Research on Cancer (IARC) has determined that hydrogen peroxide's carcinogenicity to humans is not classifiable.^[8] The advantages of using gaseous hydrogen peroxide are described by Hultman et al.⁶: 1) it will have uniform contact with all exposed surfaces, including those with complex topographies; 2) it may be safely maintained in a chamber environment; and 3) it may be efficiently and guickly removed from a chamber. Hydrogen peroxide is a strong oxidizing agent, having multiple targets within a cell as well as in almost every biomolecule: it can react strongly with thiol groups in enzymes and proteins, DNA, and the bacterial cell membrane.^[9]

Such a strong oxidizing agent can cause the formation of radicals such as ferryl radical, which is formed from DNA-associated iron and has an important role in DNA oxidation.⁹ As highlighted by the work of researchers such as Young and Setlow,^[10] Fichet et al.,^[11] and Setlow,^[12] the site of microbial inactivation by VHP appears to reside at the inner membrane.

Industrial Scale VHP

Industrial VHP sterilization chambers (Figure 1) [NOTE: Figures courtesy of STERIS] are typically one-half to four pallets (35–280 ft3). This is in contrast with large EO chambers, often ranging from 1,000 ft³ to 2,200 ft³. A distinct advantage with VHP sterilizers, however, is the minimal requirement for supplies and services: water, compressed air, electricity, and sterilant. This allows equipment to be supplied on a single skid and installed with ease, which may be advantageous for 'in-line' applications. Equipment may be commissioned and validated in a manner similar to a steam or EO sterilizer.

Limitations of VHP and the Role for Process Design

As VHP offers a number of distinct advantages, including material compatibility (as highlighted in AAMI TIR17 and Table 1 of this document), efficacious microbial inactivation, and lack of toxic residues, it does present some limitations that must be considered and addressed, namely: 1) material compatibility; 2) packaging; 3) equipment scale and throughput capability; and 4) surface penetration. Strategies to address such limitations may be summarized as follows.

Material Compatibility

VHP has a wide range of material compatibility but is limited whereby a small subset of materials must be excluded due to absorption and decomposition of the vapor. Liquids, powders, and cellulose materials are not compatible with the process.⁵

Packaging

Packaging for VHP sterilization needs to be compatible with the sterilant and allow for diffusion of the sterilant to the medical device. Packaging materials that prevent VHP from reaching the devices (e.g., foil pouches) should not be used; however, the external surfaces of the material such as glass (e.g., a liquid-containing ampoule) will be sterilized. Nonwoven polyethylene and polypropylene materials have been proposed by the Sterile Barrier Association. Such materials provide a sterile barrier for the product while allowing sterilant gases and steam to penetrate and escape quickly. Corveleyn et al.^[13] have shown that H2O2 penetration across Tyvek package was considerably greater (87.7% of reference concentration as measured inside the package) compared to that of medical paper (30%). Therefore, it is essential that devices are packed in a suitable sterile barrier.

Cellulose is associated with product packaging (cardboard) and instructions for use (paper), rather than with the medical device itself. Cellulose can absorb H2O2 to such an extent that it reduces the concentration of H2O2 in the vapor phase, causing the cycle to abort. Another potential approach might be lacquering or coating of absorbent materials like cardboard or paper.

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Meszaros et al.^[14] have examined the impact of surface material on the process lethality, and did not observe any deleterious effects with beechwood, although it is a cellulose-based material. The authors have speculated the reason might be the processed (lacquered) nature of the material. Also, as cardboard cartons must be excluded, operators may incur additional handling of materials. Possible mitigating strategies may involve the presentation of product in high-density polyethylene tote box systems: Such totes have been used in the past in EO processing to improve product residual outcomes by removing cardboard cartons from the process.

Figure 1: Picture of STERIS VHP® LTS-V



Plastics*	Metals*
Delrin ¹ (polyoxymethylene, POM) ¹	Aluminum
EVA (ethylene vinyl acetate)	Brass
KRATON ² polymers (styrenic block copolymer, SBC)	Cobalt chrome alloy
Neoprene (polychloroprene) ¹	Copper**
Noryl ³ (polyphenylene ether and ploystyrene)	Gold
Nylon ¹ (polyamide) ¹	Nitinol
PPMA (polymethyl methacrylate)	Platinum
PEEK (polyether ether ketone)	Silver
Polycarbonate, polyethylene, polypropylene, polystyrene, polyurethane	Statinless steel ¹
PVC (polyvynil chloride)	Titanium ²
Radel ⁴ (polyphenylsulfone) ¹	
Santoprene (thermoplastic vulcanizates, TPVs)	
Silicone	
Teflon ¹ (polytetrafluoroethylene, PTFE)	
Ultem ³ polymers (polyetherimide, PEI)	
Ceramics and others*	Coatings*
Alumina (Al ₂ 0 ₃)	Aluminum titanium nitride (AITiN)
Diamond, ruby, sapphire	Aluminum titanium nitride chromium Nitride (AITiN CrN)
Glass	Diamond-like carbon (DLC)
Silicone nitride (Si ₃ N ₄)	Titanium nitride (TiN)
Zirconium nitride (ZrN)	Titanium nitride titanium carbonitride (TiN TiCN)
Zirconia (Zr O_2 with or without Y_2O_3)	Tungsten carbide (WC)

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Equipment Scale and Throughput Capacity

As already described, VHP sterilizers lack large volume scale compared to EO sterilizers. However, VHP has the advantage of quicker and more efficient processing that goes some way to addressing the scale. Consequently, chamber size – coupled with additional handling requirements to exclude packaging materials – would render VHP most suitable for specific niche applications, typically at the end of production line applications. For deployment into contract sterilization offerings, supply chains must be designed to streamline product flow and handling.

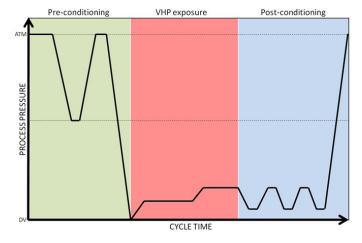
Surface Penetration

There are many different VHP sterilization processes used in the various commercial sterilizers available today, but all these processes follow a similar three-phase pattern (Figure 2): preconditioning, sterilization, and aeration. [NOTE: Figures courtesy of STERIS] First, a deep vacuum is pulled to remove air and humidity from the load and to create an environment for injecting VHP to a maximum level while not reaching the saturation point at which condensation will occur. The importance of this step is highlighted in a study performed by Hultman et al.,6 where a drop in a maximum H2O2 concentration from 2,148 to 1,805 mg/L has been reported, as moisture content goes from 0% to 10%. In the second phase, usually a 35% liquid H2O2 (w/v; pH~3) is vaporized at over 100°C and the vapor is injected into the chamber in the form of pulses to reach a final concentration of 1-2mg/L. Following sterilant exposure, vacuum is applied and using either air or steam or a combination of both to remove sterilant. Process parameters - predominantly pressure, temperature, humidity, and exposure time - can be optimized to design high-performing cycles and ensure penetration to the desired surfaces for sterilization. In lumen devices, residual air may impede vapor penetration^[15] and therefore cycle design should consider critical parameters including vacuum depth, sterilant concentration, and exposure time.

While there was previously concern about hydrogen peroxide penetration and sterilization within long narrow lumens, stainless steel and flexible lumens (e.g., flexible endoscopes) are now sterilized by subatmospheric VHP systems in healthcare. Figure 2: Diagrammatic representation of a VHP cycle showing three phases of Preconditioning, VHP exposure and Postconditioning.



Currently, there is no international standard that provides performance requirements for biological indicators for VHP sterilization processes. The process is therefore characterized in accordance with ANSI/AAMI/ISO 14937:2009/(R)2013,^[16] which states that a microorganism of known high resistance can be used to demonstrate the microbial effectiveness of the sterilizing agent. In the U.S., the FDA regulates biological indicators used in healthcare facilities and has a set of testing requirements for the clearance of VHP biological indicators in the U.S. market. While FDA 510k regulations^[17] require the use of G. stearothermophilus in the hospital setting as the most resistant organism, the 14937 standard - which is appropriate for medical device terminal sterilization applications - requires the consideration use of a biological indicator of known high resistance, similar to that as defined for EO sterilization in accordance with ANSI/AAMI/ISO 11135:2014,^[18] where Bacillus atrophaeus is the reference microrganism. It is known that G. stearothermophilus is more resistant to vapor, whereas B. atrophaeus is more resistant when subjected to liquid hydrogen peroxide^[19]. Selection of a biological indicator to challenge the process is an important step, as it consequently quantifies the microbicial inactivation of the process and therefore the process outcomes (sterility assurance and material effects).



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The validation process detailed in ISO 14937 is a familiar and accepted process, as it is very much aligned to that for EO gas sterilization18 where an overkill half-cycle approach is often adopted: Like EO validation, alternative approaches to validation are also available and may be appropriate if one is to consider a more targeted process with less overprocessing.

EO processing solicits wide acceptance from industry as it is a known, trusted technology with a long history of use. Furthermore, by nature of having its own international consensus standard (ISO 11135) recognized by the FDA, it has Category A status. VHP has Category B status, given its long history in healthcare and available body of knowledge. In 2017, a new work item was proposed to the International Organization for Standardization for the creation of a process standard for VHP sterilization. This proposal was duly accepted and a working group (WG16) formed under Technical Committee 198 (responsible for sterilization). This committee has commenced work on the draft standard, ISO/CD 22441. Similarly, in Europe work is underway by CEN TC102 WG6 to develop an equipment standard (prEN 17180) similar to EN 1422 (applicable to EO sterilizers). Once complete, both standards would provide normative references and guidance for both equipment and the sterilization processes provided by such equipment in both healthcare and industrial settings.

Conclusions

Examination of current and past applications shows VHP sterilization to be an efficacious, material-friendly, and useful sterilization technology. Like with every sterilization technology, there are limitations (described in parentheses): steam (high temperature), EO (residues), E-beam (poor penetration), gamma/X-ray (material compatibility limitations). VHP too has limitations. However, such limitations are to be considered and innovations provided to increase the adoption of the technology. Expectations for future adoption as a technology for terminal sterilization of single-use medical devices may be founded on 1) compatability with a wide range of materials, including polymers, sensors and electronics, metals, and electrical components; 2) operating temperatures typically lower than EO processing; and 3) ready deployment of selfcontained sterilization equipment. Therefore, temperaturesensitive products, sensor/electronic combination products, or those requiring sterilization at source of manufacture (e.g., 3D printed products) may be excellent candidates for such a sterilization solution.

The proliferation of any technology in medical device sterilization is predisposed to its acceptance by those who require sterilization for their manufactured devices. With continued focus, investigation, and dissemination of knowledge and experience, the possibilities VHP adds to the technology portfolio available to manufacturers can be realized. As projects are completed with a diverse range of products, experience and knowledge are gained that may be shared in future publications.

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